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Optimisation of an electronic amplifyer applied to Electrolyte/insulator/Semiconductor structures

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Abstract

This paper reports on the development of a MOSFET-based amplifier for the electrical field effect characterisation of chemical capacitors (ChemFEC) based on electrolyte/insulator/semiconductor (EIS) capacitive structures. Experimental demonstration is performed through the study of SiO_2/Si_3N_4 ion sensitive field effect capacitor (ISFEC) sensors for pH measurement. This study deals with the amplification's properties according to the ISFEC and MOSFET electrical characteristics. Thus, the ISFEC transition from the accumulation to the inversion regime is shown to be responsible for a non-linear phenomenom. Nevertheless, thanks to a compromise between the ISFEC flat band voltage and the MOSFET threshold voltage, linear responses and high detection sensitivities are evidenced on the [2 - 12] pH range. Thus, the non-linear phenomenon observed in previous works is clarified. The detection structure evidences linear responses, which is an essential parameter for sensors. Finally, high detection sensitivities are obtained on a small pH range due to this non-linearity.

Keywords: ChemFEC microsensor, MOSFET amplifier, improved detection properties

1. Introduction

The development of chemical field effect capacitors (ChemFECs), also called electrolyte/insulator/semi-conductor (EIS) sensors [1], can bring solutions in order to detect biochemical or/and biological species in liquid media. Indeed, they are somewhat simpler than chemical field effect transistors (ChemFETs) and are suited for both potentiometric or/and impedimetric detection. In return, their use requires adapted characterisation techniques. Solutions have been found either by using standard capacitance – voltage C-V measurements [2] or by developing light-adressable potentiometric sensor (LAPS) [3, 4, 5].

Another solution has proposed the development of electronic amplifiers adapted to the ChemFEC characterisation. It has lead to the study of a ChemFEC/MOSFET amplifier [6]. Thus, theoretic calculations and simulations have shown the potentialities of this amplifier for improving the detection properties of field-effect chemical sensors, taking into account static and dynamic phenomena [7]. However, even if improved detection sensitivities have been evidenced experimentally for the pH measurement, results have still exhibited an unclear non-linear phenomenom [6].

This paper deals with the study of the ChemFEC/MOSFET amplifier and aims to explain the pH detection non linear phenomenom through the experimental comparison of different ChemFEC chemical sensors and of different metal/oxide/semiconductor field effect transistors (MOSFET).

2. Experimental

The pH-sensitive field-effect capacitors (pH-ISFECs) were fabricated on <100>oriented, P-type (3-5 Ω .cm) silicon substrate. The ionosensitive gate was formed using a silicon nitride Si₃N₄ layer deposited on top of a thermally grown silicon dioxide SiO₂ layer (figure 1). Special attention was given for obtaining high capacitance values by increasing the capacitor area. The chemical sensors were formed on a chip designed with a specific geometry (about 8 millimetres long, 2.6 millimetres wide and 0.5 millimetre thick) (figure 2). Finally, the pH-ISFEC chips were stuck on printed circuit thanks to an insulating epoxy glue. After wire bonding and coating, encapsulation was performed using a silicone, leaving the sensitive parts uncovered (figure 3). All in all, two different pH-ISFEC sensors were fabricated for comparison (table 1).

In the following, the pH-ISFECs will be modelled by the association of an equivalent capacitor C_{th} and a voltage source E_{th} (figure 4). E_{th} represents the potential drop in the electrolyte at the insulator/electrolyte interface. According to the Nernst law, it can be related to the solution hydrogen potential pH as following [8]:

$$E_{th} = s_0(pH_{pzc} - pH)$$
(1)

where pH_{pzc} is the pH at the point of zero charge, estimated around 4 for silicon nitride Si₃N₄ [9, 10], and s₀ is the ISFEC sensitivity to pH, experimentally estimated around 55 mV/pH.

In order to study the influence of the pH-ISFEC characteristics on the behaviour of the ChemFET/MOSFET amplifier, two different MOSFET transistors, i.e. PMOS and NMOS type (table 2) were studied. Thus, two amplifying structures have been realised in order to keep a positive bias on the pH-ISFEC capacitor (figures 5 and 6). In both cases, the MOSFET transistor was biased by a KEITHLEY 220 current source (bias current: $I_0 = 50 \mu A$) and the drain-source voltage V_{DS} variations with time was recorded thanks to a Tektronics TDS 220 oscilloscope. For all characterisation experiments, source voltages were applied to the solution using a reference calomel electrode.

Test solutions were realised by diluting hydrochloric acid HCl and tetramethylammonium hydroxide (TMAH) N(CH₃)₄OH with pure water. Solution pH were estimated by a ORION 710A digital pH-meter with a precision of \pm 0.01 pH unit after

calibration with three standard buffer solutions (pH = 4.01, 7.00 and 10.01). All the measurements were done at a constant temperature $(20^{\circ}C)$.

3. Comparison of the pH-ISFEC/MOSFET structures

The theoretic study of the ChemFEC/MOSFET amplifier has been described elsewhere [6]. Here will be only compared the PMOS and the NMOS amplifier applied to our capacitive sensor.

For the NMOS amplifier (figure 5), considering that the gate voltage V_G is constant and that the gate current I_G is negligible [6], the drain voltage V_D is given by:

Since the drain voltage V_D is positive and taking into account equation (1), it can be written:



For the PMOS amplifier (figure 6) and with the same assumptions than previously, the drain voltageV_D is given by:

(4)

Since the drain voltage V_D is negative and always taking into account equation (1), it can be written:

(5)

(2)

Therefore, from equations (3) and (5), the absolute value of the drain voltage follows similar variations with pH whatever the amplifier type. This parameter will therefore be studied hereafter.

4. Results and discussion

Related to the previous study [6], variations of the voltage V_{max} have been plotted as a function of solution pH for several capacitances C (figure 7). These results have been obtained with the ISFEC #1 (table 1) and the PMOS transistor (table 2).

Non-linear curves are evidenced whatever the value of C for a pH value around 4. In order to explain this non-linear phenomenon, different assumptions, either related to dynamic effects, either related to the chemical properties of the Si₃N₄ ionosensitive film chemical properties, were proposed and discarded [6].

From another point of view, the non-linearity could be related to the ISFEC transition from the accumulation regime to the inversion one. Indeed, since the V_{GS} voltage is assumed to be constant, roughly equal to the MOSFET threshold voltage V_T [6], the variations of the pH value induce variations on the ISFEC voltage V.

Thanks to this last assumption and using the electric model of the pH-ISFEC (figure 4) and the PMOS amplifier (figure 6), the non-linear phenomenon observed on figure 7 allows an estimation of the ISFEC #1 flat-band voltage V_{FB} :



We therefore obtain a good agreement with the flat-band voltage value determined using quasi-static capacitance-voltage C(V) experiments on the ISFEC#1 capacitor (Table 1).

To complete the study, the ISFEC #1 has been studied using the NMOS amplifier (figure 5) with the corresponding NMOS transistor (table 2). In this case, linear curves are therefore observed on the [2 - 12] pH range (figure 8). In fact, if the non-linear phenomenon is related to the ISFEC accumulation - inversion transition, a simple calculation gives the pH value where it should appear:

		(7)
else:		

This pH value is clearly impossible and therefore the non-linear phenomenon cannot be evidenced in the tested configuration.

The second generation of ISFEC sensors allows checking again the influence of the ISFEC accumulation - inversion transition. Figure 9 shows the NMOS amplifier output characteristics using an ISFEC#2 sensor (table 1). Again, non-linear phenomena are evidenced, this time around pH = 8.5. Firstly, this pH shift between figures 7 and 9 demonstrates definitively that the non-linearity is not related to pH_{PZC} value [6]. Secondly, this result should allow to determine the ISFEC#2 flat-band voltage V_{FB}:



Again, a good agreement is obtained with the flat-band voltage value determined using quasi-static capacitance-voltage C(V) experiments on the ISFEC#2 capacitor (Table 1).

To check a last time our assumption, the ISFEC#2 has been tested using the PMOS amplifier (figure 6). Thus, by shifting the ISFEC voltage range, we obtain again linear curves on the [2 - 12] pH range (figure 10). Indeed, in this last case, the pH value giving the non-linear-phenomenon can be estimated to a non-realistic value:



Finally, the amplification ratio r has been studied as a function of the capacitance ratio $C_{Th}/(C+C_{GD})$ (figure 11). Whatever the ISFEC/MOSFET amplifier chosen, a linear relation is evidenced in agreement with previous results [7].

5. Conclusions

MOSFET-based amplifier symmetry have been studied whatever the MOS transistor type. The non-linear phenomenon evidenced in some case has been related to the ISFEC transition from the accumulation to the inversion regime. This effect has been tackled off by choosing in an optimal way the MOSFET threshold voltage and, thus, by discarding the ISFEC flat-band voltage value from the ISFEC voltage range on the [2 - 12] pH range (equation 1). Therefore, whatever the ISFEC tested, a compromise on the amplifier will be always possible in order to reach linear responses and high detection sensitivities.

Nevertheless, non-linear effects could be interesting for any applications working on small pH ranges such as medical ones. Indeed, zooming on figure 9, the non-linear phenomenon offers a very high sensitivity (3.5 V/pH) for pH around 8. Furthermore, as the non-linearity is due to the capacitive structure, sensitivity could be still increased by modifying the doping profile of ISFEC sensors. Thus, by adjusting the compromise between the MOSFET type and the ISFEC flat-band voltage, it should be possible to obtain an optimal sensitivity on specific detection range.

References

- [1] D.R. Thévenot, K. Toth, R.A. Durst, "Electrochemical biosensors: recommended definitions and classification", *Biosensors & Bioelectronics*, 16 (2001), 121-131
- [2] F. Chauvet, A. Amari, A. Martinez: "Stability of silicon nitride/silicon dioxide/silicon electrodes used in pH microelectronic sensors", *Sensors and Actuators*, Vol.6 (1984), 255
- [3] D. Hafeman, J. Parce, H. McConnell: "Light-addressable potentiometric sensor for biochemical systems", *Science*, 240 (1988), 1182-1185
- [4] A. Ismail, H. Sugihara, T. Yoshinobu, H. Iwasaki: "A novel low-noise measurement principle for LAPS and its application to faster measurement of pH", *Sensors and Actutors*, B 74 (2001), 112-116
- [5] G. Ferri, P. De Laurentiis, A. D'Amico, C. Di Natale: "A low-voltage integrated CMOS analog lock-in amplifier prototype for LAPS applications", *Sensors and Actuators*, A 92 (2001), 263-272

- [6] P. Temple-Boyer, J. Launay, G. Sarrabayrouse, A. Martinez: "Study of capacitive structures for amplifying the sensitivity of FET-based chemical sensors", *Sensors and Actuators*, B78 (2001), 285-290
- [7] P. Temple-Boyer, J. Launay, G. Sarrabayrouse, A. Martinez: "Amplifying structure for the development of field effect capacitive sensors", *Sensors and Actuators*, B4318 (2002), 1-11
- [8] L. Bousse, N.F. De Rooij, P. Bergveld: "Operation of chemically sensitive field effect sensors as a function of the insulator-electrolyte interface", *IEEE Transactions on Electron Devices*, ED30 (1983), 1263
- [9] M. Grattarola, G. Massobrio, S. Martinoia: "Modeling H⁺-sensitive FET's with SPICE", *IEEE Transactions on Electron Devices*, ED39 (1992), 813
- [10] A.A. Poghossian: "Determination of the pHpzc of insulators surface from capacitancevoltage characteristics of MIS and EIS structure", *Sensors and Actuators*, B 44 (1997), 551-553

Biographies

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Pierre Temple-Boyer was born the 25th of October 1966. He received the degree in electronic engineering from the Ecole Supérieure d'Electricité (Paris – France) in 1990. He joined the Laboratoire d'Architecture et d'Analyse des Systèmes from the french Centre National de la Recherche Scientifique (LAAS-CNRS) in 1992 and received the PhD degree from the Institut National des Sciences Appliquées de Toulouse (France) in 1995. Since then, as a senior researcher, he has been working on the development of micro- and nanotechnologies.

FIGURE CAPTIONS

Figure 1: structure of the pH-ISFEC

Figure 2: picture of the pH-ISFEC silicon chip

Figure 3: silicone ecapsulation

Figure 4: electric model of the pH-ISFEC

Figure 5: schematic of the NMOS amplifier

Figure 6: schematic of the PMOS amplifier

Figure 7: voltage V_{max} as a function of solution pH for different capacitances C $(C_{th} = 1.9 \text{ nF} / V_T = -1.4 \text{V})$

Figure 8: voltage V_{max} as a function of solution pH for different capacitances C $(C_{th} = 1.9 \text{ nF} / V_T = 0.8 \text{V})$

Figure 9: voltage V_{max} as a function of solution pH for different capacitances C $(C_{th} = 1.5 \text{ nF} / V_T = 0.8V)$

Figure 10: voltage V_{max} as a function of solution pH for different capacitances C $(C_{th} = 1.5 \text{ nF} / V_T = -1.4 \text{V})$

Figure 11: amplification ratio r as a function of the capacitance ratio $C_{TH}/(C+C_{GD})$

Figure 12: high sensibility due to thenon-linear phenomenon

Table 1: ISFEC characteristics

Table 2: MOSFET characteristics



Figure 1: structure of the pH-ISFEC



Figure 2: picture of the pH-ISFEC silicon chips



Figure 3: silicone encapsulation of the pH-ISFECs



Figure 4: electrical model of the pH-ISFEC



Figure 5: schematic of the NMOS amplifier



Figure 6: schematic of the PMOS amplifier



Figure 7: voltage V_{max} as a function of solution pH for different capacitances C

 $(C_{th} = 1.9 \text{ nF} / V_T = -1.4 \text{V})$



<u>Figure 8: voltage V_{max} as a function of solution pH for different capacitances C</u>

 $(C_{th} = 1.9 \text{ nF} / V_T = 0.8 \text{V})$



Figure 9: voltage V_{max} as a function of solution pH for different capacitances C

 $(C_{th} = 1.5 \text{ nF} / V_T = 0.8V)$



<u>Figure 10: voltage V_{max} as a function of solution pH for different capacitances C</u>

 $(C_{th} = 1,5 \text{ nF} / V_T = -1,4V)$



Figure 11: amplification ratio r as a function of the capacitance ratio $C_{th}/(C+C_{GD})$



Figure 12: high sensibility due to the non-linear phenomenon

ISFEC type	Gate structure	Gate surface	Gate capacitance	Flat-band voltage
				V_{FB}
# 1	SiO ₂ / Si ₃ N ₄	4 mm^2	1.9 nF	$\approx 1.2 \text{ V}$
	(50nm / 50nm)			
# 2	SiO ₂ / Si ₃ N ₄	2 mm^2	1.5 nF	$pprox 0.4 \ V$
	(30nm / 30nm)			

Table 1: ISFEC electrical characteristics

MOSFET type	Threshold voltageV _T (V)	Drain-Source capacitance C _{GD}
PMOS	- 1.4 V	40 pF
NMOS	+ 0.8 V	25 pF

Table 2: MOSFET electrical characteristics