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Evaluation of Cell Membrane Effects after 3D Multicellular Spheroids RF Exposure

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Abstract— Herein we present the assessment of RF-induced cell membrane effects assessment in multicellular spheroids, which are three-dimensional tissue models resembling small avascular tumors. The RF exposure was performed in a dedicated RF applicator, which allowed a precise RF metrology as well as calibrated and systematized conditions of application of electromagnetic fields to multiple 3D multicellular spheroids. The used RF micro-device allowed us varying different RF parameters (such as frequency, power, or modulation) in order to evaluate RF-related biological effects on the membranes of cells constituting the multicellular spheroids. The effects of electromagnetic signals were assessed on cancer cells spheroids made with HCT-116 cells. Appraised parameters included the evaluation of cell membrane integrity, and the assessment of spheroids global structure after illumination. After RF exposure at Specific Absorption Rate values ranging from 0.4 to 37 kW/kg (attaining a thermal increment ΔT_{\max} up to 6°C), we did not observe any detrimental effects on the membrane level. Moreover, the spheroids exhibited an unmodified architecture.

Keywords— *microwave, micro-technologies, RF effects, biological effects, cell membrane, cell organelles, micronucleus, 3D cellular models*

I. INTRODUCTION

The biological effects that might be induced by radiofrequency (RF) radiation attract considerable scientific and public attention. The main open questions are whether or not RF radiation can be harmful and what the RF-exposure thresholds are. In order to answer these questions, it is necessary to design exposure systems, allowing calibrated and systematized

conditions of application of electromagnetic fields. In this context, we developed a calibrated RF micro-device working in a near field configuration and tested it using different RF parameters (such as frequency, power, or modulation), in order to evaluate RF-related biological effects. Unlike classical devices, where living cells are illuminated in 2D cultures, mainly with far field test setups [1]-[5], we herein present the use of a RF applicator, which allows RF-exposure of 3D multicellular spheroids.

This 3D model provides many assets: it combines the advantages of both 2D cells culture model and *in vivo* testing with an easy access to various cell lines, a rapid growth, at a limited and affordable cost, as well as a more important complexity, which is more relevant of the living, while avoiding *in vivo* testing. Cancer cells multicellular spheroids thus represent a 3D micro-tissue model, which resemble small avascular tumors. Moreover, spheroids may also be compatible with miniature RF exposure systems using micro-technologies.

The device which was used in this study allows a simultaneous illumination of five multicellular spheroids. The exposure system thus allows a high throughput analysis of potential biological effects, induced by RF electromagnetic signals, resembling to the ones used in Bluetooth or wireless technology.

II. ARCHITECTURE OF THE RF APPLICATOR NETWORK AND ASSOCIATED TECHNOLOGY

A miniature RF applicator suitable for illuminating micro-tissues was developed. The device consists of a coplanar waveguide ended by a capacitive patch. The latter is crossed by a microfluidic channel, which includes a specific area dedicated to the micro-tissue localization. This channel is associated to two

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reservoirs placed apart, maintaining the micro-tissue within its culture medium during RF exposures duration. This structure is fully electromagnetically characterized. Its experimental dosimetry study may be found in [6] as well as the exposure test bench.

In order to allow a sufficient statistical evaluation of electromagnetic fields impact on cells and due to its miniature size, the structure was adapted to enable the simultaneous RF illumination of five micro-tissues. This network configuration is shown in Fig. 1. Micro-tissues are located within each fluidic reservoir, which are drawn in pink color on the schematic, at the end of small length coplanar lines. A main coplanar waveguide (drawn in blue color) is used to feed the five RF applicators. Due to the coplanar configuration of the waveguides, metallic bridges for ground balancing are required at the input of each RF applicator. Fig. 2 presents a zoomed view of one RF applicator, which integrates the micro-tissue area above the capacitive patch.

To realize such a structure, the technological process is performed in 4 main steps. The coplanar lines are first fabricated with a lift-off process and using a thin seed layer of titanium followed by a 0.3 μm thick gold layer. A bio-compatible polymer layer is then patterned to isolate the micro-tissue from the metallic layer. An additional metallic layer is subsequently patterned on top to avoid any ground unbalance at the intersection of the RF applicator feed lines and the main coplanar waveguide. Finally, the high fluidic walls are fabricated with a 500 μm thick polymer layer to realize the fluidic reservoir and channels.

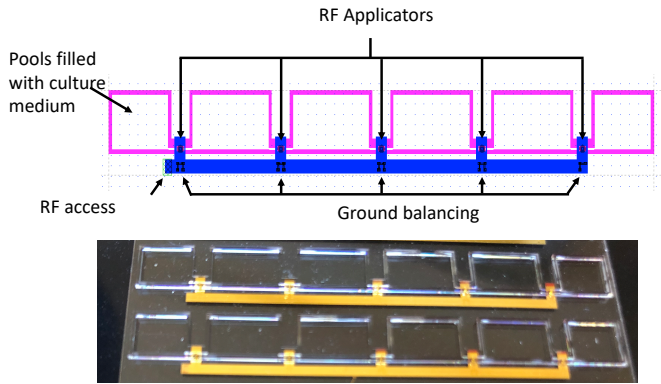


Fig. 1. Schematic and photography of the RF applicators network associated to culture medium pools.

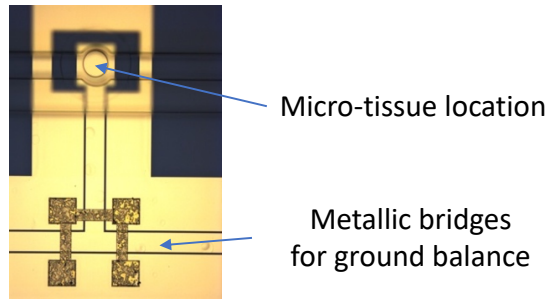


Fig. 2. Zoomed view of a RF applicator for micro-tissue with metallic bridges used for ground balancing along the principal coplanar waveguide.

The RF exposure setup, composed of an RF source is then connected to the coplanar structure using a cable and a coplanar probe.

Such a structure, implying non-sub-wavelength transmission lines connected to sensing capacitors, presents stationary waves at 2.45 GHz. This translates into different maximum electrical fields developed in each capacitor and consequently different Specific Absorption Rate – SAR - values for each micro-tissue location.

III. BIOLOGICAL EFFECTS AFTER MULTICELLULAR SPHEROIDS RF EXPOSURE : FOCUS ON CELL MEMBRANE INTEGRITY

Multicellular spheroids were exposed to RF signals in continuous waves (CW) at 2.45 GHz. The exposure lasted 5 minutes, after which we examined the cell membrane integrity of cells constituting multicellular spheroids. This procedure involved the use of propidium iodide (PI), a small molecular probe, which has an increased fluorescence yield after penetration into the cell. The PI penetration can occur when the cell membrane is damaged, such as in cases when spheroids are exposed to short and intense electric field pluses, which were applied to the positive control as previously described [7].

Different conditions were applied to spheroids in order to ensure the results. Positive controls consisted in spheroids treated with pulsed electric field (eight pulses lasting 100 μs , which were delivered with stainless steel parallel plate electrodes, at a frequency of 1 Hz and field intensity of 1.3 kV/cm), and thus presented membrane defects. Negative control were untreated spheroids, whereas sham were spheroids that were placed in the device but were not illuminated. Finally, RF-exposed spheroids were illuminated within the RF micro-device.

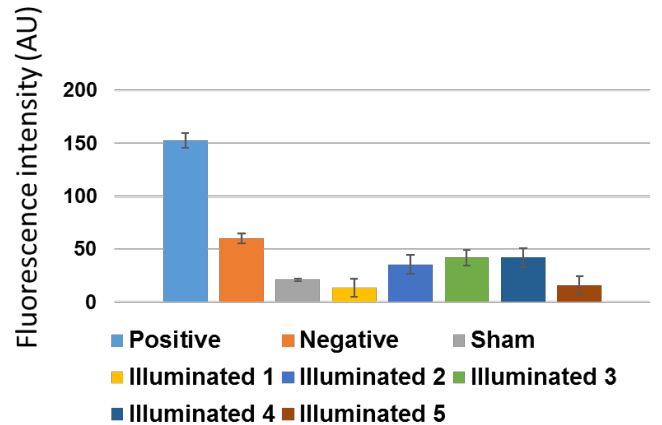


Fig. 3. Fluorescence intensity quantification after propidium iodide (PI) intake following five minutes RF-exposure (in CW mode) of HCT-116 multicellular spheroids.

The numbers 1 to 5 denote the position within the applicator, with position No 4 correlating with the lowest SAR (0.43 kW/kg for a source power of 33 dBm) and position No 2 correlating with the highest SAR (7.5 kW/kg for a source power of 33 dBm). The graph shows the mean values and corresponding standard deviations, while $N_{\text{positive}} = 3$, $N_{\text{negative}} = 5$, $N_{\text{sham}} = 4$, $N_{\text{illuminated}} = 5$ per position within the micro-device. Fig. 3

presents the fluorescence intensity quantification after propidium iodide (PI) intake following five minutes RF-exposure (in CW mode) of HCT-116 multicellular spheroids as well as for the different control configurations. Under our experimental conditions, RF signals did not alter the integrity of cell membranes (Figure 3), which resulted in lower fluorescence intensity of illuminated spheroids in comparison to the positive control.

Representative cancer cells spheroids fluorescence is shown in Fig. 4, where A) corresponds to the positive control treated with pulsed electric field (eight pulses lasting 100 μ s, which were delivered with stainless steel parallel plate electrodes, at a frequency of 1 Hz and field intensity of 1.3 kV/cm), B) is a sham placed in the device but not illuminated, and C) is a spheroid illuminated at the highest SAR (7.5 kW/kg for a source power of 33 dBm).

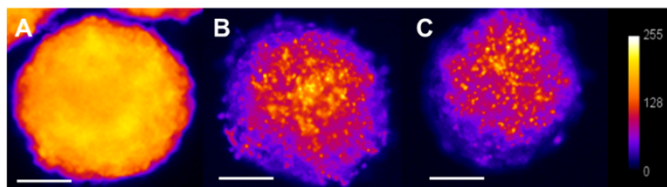


Fig. 4. Fluorescence micrographs of representative multicellular spheroids. The fluorescence is represented in a pseudo-color scale (fire scale obtained by the ImageJ software). Scale bar: 100 μ m.

After RF exposure, the multicellular spheroids remained spherical (Fig. 4). The cells forming the spheroids did not detach, and we did not observe any membrane blebs on the outer rim of the micro tissue.

IV. CONCLUSIONS

In the present work, we present the assessment of the impact of RF signals exposure on cell membrane integrity. This is enabled with the combination of both a multi-spheroid RF applicator specifically developed and a strict biological protocol applied to several illuminated micro-tissues and controls. Under exposure conditions described herein, we did not observe any alterations in cell membrane permeability. Moreover, RF exposure did not alter spheroids architecture. Additional tests will be performed to assess any potential damage on cell organelles.

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